



Assessment of phase-lag entropy, a new measure of electroencephalographic signals, for propofol-induced sedation

Mi ROUNG Jun¹, Jae Hwa Yoo², Sun Young Park², Sojin Na², Hyerim Kwon², Jae-Hwi Nho³, and Soon Im Kim²

¹Department of Anesthesiology and Pain Medicine, Samsung Changwon Hospital, Sungkyunkwan University School of Medicine, Changwon, ²Departments of Anesthesiology and Pain Medicine, ³Orthopedic Surgery, Soonchunhyang University Seoul Hospital, Seoul, Korea

Background: Phase-lag entropy (PLE) was recently described as a measurement of temporal pattern diversity in the phase relationship between two electroencephalographic signals from prefrontal and frontal montages. This study was performed to evaluate the performance of PLE for assessing the depth of sedation.

Methods: Thirty adult patients undergoing upper limb surgery with a brachial plexus block were administered propofol by target-controlled infusion. The depth of sedation was assessed using the Observer's Assessment of Alertness/Sedation (OAA/S) scale. The effect-site concentration (C_e) of propofol was initially started at 0.5 $\mu\text{g/ml}$ and was increased in increments of 0.2 $\mu\text{g/ml}$ until an OAA/S score of 1 was reached. Three minutes after the target C_e was reached, the PLE, bispectral index (BIS), and level of sedation were assessed. Correlations between the OAA/S score and PLE or BIS were determined. The prediction probabilities (P_k) of PLE and BIS were also analyzed.

Results: The PLE values were closely correlated with the OAA/S scores (Spearman's $\rho = 0.755$; $P < 0.001$) to an extent comparable with the correlation between the BIS and OAA/S score (Spearman's $\rho = 0.788$; $P < 0.001$). The P_k values of PLE and BIS were 0.731 and 0.718, respectively.

Conclusions: PLE is a new and reliable consciousness monitoring system for assessing the depth of sedation induced by propofol, which is comparable with the BIS.

Keywords: Consciousness monitor; Electroencephalography; Propofol; Sedation.

Corresponding author: Soon Im Kim, M.D., Ph.D.
Department of Anesthesiology and Pain Medicine, Soonchunhyang University Seoul Hospital, 59 Daesagwan-gil, Yongsan-gu, Seoul 04401, Korea
Tel: +82-2-709-9302, Fax: +82-2-790-0394
Email: anesikim@gmail.com
ORCID: <https://orcid.org/0000-0001-8884-4096>

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Introduction

It is important to measure the level of consciousness during general anesthesia to reduce the possibility of awareness, avoid overdoses, and improve patient outcomes. Monitoring is also essential for sedative titration to maintain adequate sedation. Therefore, several electroencephalography (EEG)-based devices are widely used to monitor the depth of anesthesia.

Recent reports have emphasized that the conscious state is associated with a rich repertoire of brain network activity and that brain functional connectivity patterns are diminished under anesthesia [1-3]. In functional magnetic resonance imaging

studies, structured long-range connectivity remains in the unconscious state, whereas the rich repertoire of diverse functional configurations seen during consciousness is disrupted under general anesthesia [1]. Despite evidence that anesthesia alters the spatiotemporal dynamics of neural activity corresponding to the loss of consciousness, most current conventional monitoring systems are dependent on the amplitude of a single-channel electroencephalogram or spectral analysis (including biphasic analysis), thereby ignoring information related to dynamic connectivity [4]. A popular method used to infer connectivity among brain regions is phase synchronization with coherency or phase locking. This method requires stationary data with a rather long time series (several seconds) to reliably estimate the strength of functional connectivity [5,6].

A phase-lag entropy (PLE) monitor (PLEM100; InBody Co., Korea) was recently introduced as a device to monitor the conscious state by measuring electroencephalographic signals and calculating PLE. Importantly, PLE is a new framework that predicts the complexity of communication by calculating the diverse connectivity of temporal patterns in phase relationships between two electroencephalographic signals from prefrontal and frontal montages, rather than the strength of phase coupling, as reflected in classical techniques. A high correlation has been reported between PLE and the level of consciousness [7].

This study was performed to investigate the ability of PLE to assess the level of sedation, as measured by the Observer's Assessment of Alertness/Sedation (OAA/S) scale, during propofol-induced sedation in patients undergoing upper limb surgery with a brachial plexus block. We simultaneously compared PLE with the bispectral index (BIS), the most commonly used parameter to monitor the level of consciousness.

Materials and Methods

Patient population

This study was approved by the Institutional Review Board of our hospital (Ref. 2017-05-018) and was registered with the International Clinical Trials Registry Platform (<http://cris.nih.go.kr>). Thirty patients (aged ≥ 18 years, American Society of Anesthesiologists physical status I or II) scheduled for elective upper limb surgery under a brachial plexus block were recruited between July and September, 2017. Written informed consent was obtained from all patients on the day before the operation. Patients were excluded for the following reasons: the presence of neurological, hepatic, or renal disease; a history of obstructive sleep apnea; body mass index ≥ 30 kg/m²; a history of adverse drug reactions to propofol or local anesthetics; a history of an allergic reaction to soybeans; or pregnancy. Patients who were on medications that affect the central nervous system (CNS) (e.g.,

anticonvulsants, hypnotics, and analgesics) were also excluded from the study.

Study procedure

When patients arrived at the operating room, noninvasive arterial blood pressure, electrocardiography, and peripheral oxygen saturation monitoring were initiated. An ultrasound-guided brachial plexus block was performed via the axillary approach. Next, 20 ml of 0.45% ropivacaine were administered after negative aspiration and adequate sensory block was confirmed at 15 min after the injection of local anesthetics. In addition, CNS symptoms (e.g., feelings of lightheadedness and dizziness, visual and auditory disturbances, disorientation and occasional feelings of drowsiness, shivering, muscular twitching, tremors, and generalized convulsions of a tonic-clonic nature before propofol infusion) caused by the local anesthetics were observed and recorded. Disposable PLE and BIS sensors were placed on each patient's forehead, as recommended by the manufacturer, and connected to the PLE and BIS monitor (BIS[®] Monitor; Medtronic, Ireland), respectively. Baseline PLE and BIS values were recorded. The effect-site concentration (C_e) of propofol was initially started at 0.5 $\mu\text{g/ml}$ via a target-controlled infusion pump (Orchestra[®] Base Primea; Fresenius Vial, France) using Schnider's pharmacokinetic model [8]. During the study period, the level of sedation was assessed by one investigator using the OAA/S scale (5 = responds readily to name spoken in normal tone; 4 = lethargic response to name spoken in normal tone, 3 = responds only after name is called loudly or repeatedly, 2 = responds only after mild prodding or shaking, 1 = does not respond to mild prodding or shaking) [9].

The C_e was increased in increments of 0.2 $\mu\text{g/ml}$ until an OAA/S score of 3 was reached, and then in increments of 0.1 $\mu\text{g/ml}$ until an OAA/S score of 1 was reached (loss of consciousness). Three minutes after the target C_e was reached, the PLE and BIS values, blood pressure, heart rate, and peripheral oxygen saturation were recorded, and the investigator evaluated the level of sedation. Oxygen was administered at 5 L/min via a face mask until the end of the operation.

The primary goal of this study was to determine the correlation between the PLE values and the propofol-induced sedation level, as evaluated by the OAA/S scale, in comparison with the BIS values. Secondary goals were to compare PLE with the BIS value through prediction probability, and to examine the pharmacodynamic relationship between the sedation level and the C_e of propofol for each OAA/S score.

Statistics

Nonparametric Spearman correlation analysis was used to

determine correlations between the OAA/S score and the PLE or BIS value. The PLE and BIS values were compared using the Wilcoxon matched-pairs signed-rank test or Student's *t*-test. Continuous variables are shown as means ± standard deviations (SDs) or medians (25th–75th percentiles), while categorical variables are expressed as integers. All statistical analyses were performed using SigmaStat software, version 3.5 for Windows (Systat Software, Inc., USA). In all analyses, *P* < 0.05 was considered to indicate statistical significance.

P_k values were calculated using Somers' d cross-tabulation statistic to evaluate the performance of the monitor [10]: *P_k* = 1 indicates that the measure predicts the observed depth of anesthesia perfectly; *P_k* = 0.5 indicates that the predictive accuracy of the measure is no better than chance (50 : 50); and *P_k* = 0 indicates that the measure has no predictive value.

Probability of sedation and pharmacodynamic analysis

The following sigmoid Emax model was used to determine the relationship between the probability of sedation (*P*) and *C_e* of propofol:

$$P(\text{sedation} \leq \text{OAA/S score of } i) = \frac{C_e^r}{C_{e50_OAA/S \text{ score of } i}^r + C_e^r}$$

where *C_{e50_OAA/S score of i}* is the *C_e* associated with a 50% sedation probability ≤ the *i*th OAA/S score, and *γ* is the slope of the concentration versus the sedation probability curve. Model parameters were estimated using the option 'LIKELIHOOD LAPLACE METHOD = conditional' in NONMEM® 7 level 3 (ICON Development Solutions, Ireland). IIV of the *C_{e50}* was fixed at zero.

Results

We collected 315 data points from 30 patients; the patients' characteristics are summarized in Table 1. There were no signs of CNS toxicity due to local anesthetics during the brachial plexus block. During propofol-induced sedation, no significant

Table 1. Patient Characteristics

Variables	Data values
Age (yr)	53.6 ± 14.8
Sex (M/F)	15/15
Body mass index (kg/m ²)	23.8 ± 2.7
Lean body mass (kg)*	48.5 ± 7.6
ASA physical status (I/II)	19/11

Values are presented as mean ± SD or number of patients. ASA: American Society of Anesthesiologists. *Janmahasatian formula [22].

adverse events requiring cardiovascular or respiratory support occurred.

With increasing depth of sedation, the PLE and BIS values decreased progressively. As the OAA/S score decreased from 5 to 1, the median values (25th–75th percentiles) of PLE and BIS decreased from 85 (79–89) to 59.5 (54–65) and from 88 (83–93) to 60.5 (54–63), respectively (Fig. 1). PLE was closely correlated with the OAA/S score that was similar to the correlation between the BIS value and OAA/S score during propofol-induced sedation (Spearman's Rho = 0.755 and 0.788, respectively; both *P* < 0.001).

The *P_k* values (95% CI) of PLE and BIS were 0.731 (0.708–0.754) and 0.718 (0.696–0.740), respectively.

The pharmacodynamic model parameters and logistic regres-

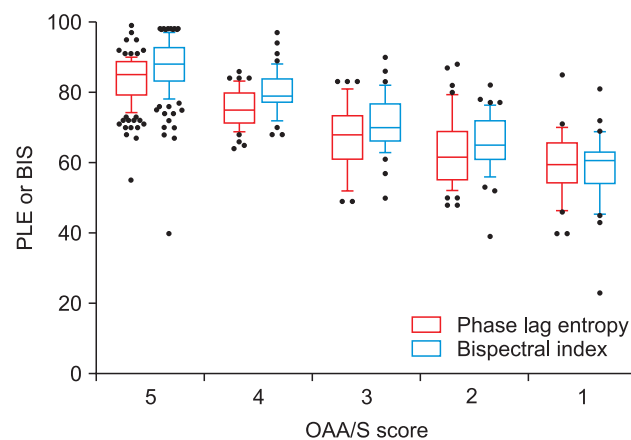


Fig. 1. Box and whiskers plot (10th, 25th, 50th, 75th, and 90th percentiles) of phase-lag entropy (PLE) or the bispectral index (BIS) at each Observer's Assessment of Alertness/Sedation (OAA/S) score. As the OAA/S score decreased from 5 to 1 (i.e., 5 → 4 → 3 → 2 → 1), the median values (25th–75th percentiles) of PLE and BIS gradually decreased from 85 (79–89) to 75 (71–79.8) to 68 (61.8–74) to 61.5 (55–69) to 59.5 (54–65), and from 88 (83–93) to 79 (77–83.8) to 70 (66–77) to 65 (61–72) to 60.5 (54–63), respectively. The OAA/S score was closely correlated with PLE to an extent comparable with that of the BIS during propofol-induced sedation (Spearman's Rho = 0.755 and 0.788, respectively; *P* < 0.001).

Table 2. Pharmacodynamic Model Parameters for Each OAA/S Score

Parameter	Estimate (% RSE)
<i>C_{e50_OAA/S score of 1}</i>	2.69 (4.24)
<i>C_{e50_OAA/S score of 2}</i>	2.22 (3.35)
<i>C_{e50_OAA/S score of 3}</i>	1.96 (3.27)
<i>C_{e50_OAA/S score of 4}</i>	1.67 (2.76)
<i>γ</i>	9.56

OAA/S: Observer's Assessment of Alertness/Sedation, *C_{e50_OAA/S score of n}*: effect-site concentration associated with a 50% sedation probability ≤ the *i*th OAA/S score, *γ*: steepness of the concentration versus response relationship, RSE: relative standard error.

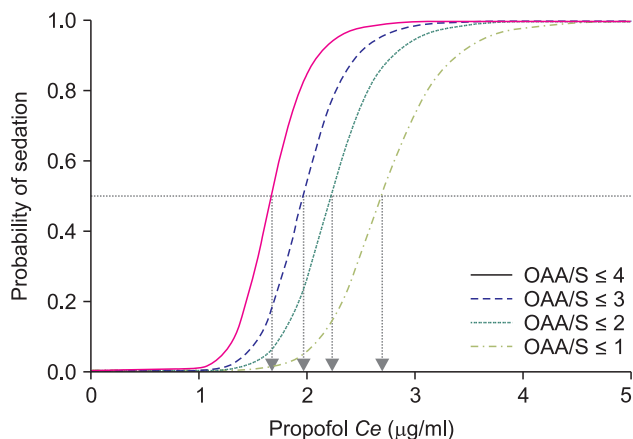


Fig. 2. Relationship between the probability of sedation and the C_e of propofol at each Observer's Assessment of Alertness/Sedation (OAA/S) score. The C_{e50} (arrow) values were estimated to be 1.67, 1.96, 2.22, and 2.69 $\mu\text{g/ml}$ for OAA/S scores of ≤ 4 , ≤ 3 , ≤ 2 , and ≤ 1 , respectively.

sion curve depicting the relationship between the C_e of propofol and the probability of sedation at each OAA/S score are shown in Table 2 and Fig. 2, respectively. The C_{e50} values were estimated to be 1.67, 1.96, 2.22, and 2.69 $\mu\text{g/ml}$ for OAA/S scores of ≤ 4 , ≤ 3 , ≤ 2 , and ≤ 1 , respectively.

Discussion

This study demonstrates that PLE was closely correlated with the level of sedation measured by the OAA/S score. The ability of PLE to assess the depth of sedation was comparable with that of the BIS value. Recent studies suggest that the state of consciousness is more closely associated with the temporal dynamics of the functional network configuration among brain areas, rather than with the strength of static connectivity [1,3,11]. Lee et al. [7] revealed that the conscious state consists of diverse patterns of functional connectivity, whereas the anesthetized state has a few dominant patterns, suggesting stereotypic communication. However, current techniques for measuring connectivity in brain regions do not adequately explain the temporal dynamics of neurophysiological signals. Popular methods that use phase synchronization [5,6] assume stationarity throughout the measurement period. The phase synchronization value is obtained by averaging phase differences across periods of several seconds, and important temporal information can be lost. Most EEG-based systems for monitoring the depth of anesthesia, including BIS, use this mechanism. Additionally, most such systems consider only the temporal characteristics of single-channel EEG, thereby disregarding spatial or connectivity information [4].

Unlike previous monitoring methods, PLE can be used to successfully evaluate the diversity of connectivity patterns,

measured on time scales of tens of milliseconds, and to more accurately track the state of consciousness, compared with static strength-based connectivity. PLE quantifies the diversity of temporal patterns in the phase relationship between two signals and then incorporates the temporal dynamics of the instantaneous phase time series into the phase synchronization analysis. Therefore, PLE exhibits better performance when classifying states of consciousness, compared with a classical time-averaged connectivity method [12–14]. Anesthesia suppresses diverse connectivity patterns in brain activity [15–17]. The increased synchronization due to anesthesia is reinterpreted as a stereotypic communication and exhibits a substantial decrease in PLE, suggesting impairment in flexible corticocortical communication. Among several depth of anesthesia indicators studied recently, PLE exhibited the highest agreement with the level of consciousness [7]. The other indicators assessed only the temporal features of single-channel EEG and therefore dismissed spatial relationships across cortical areas; these relationships have critical relevance to the states of consciousness [11,12].

In this study, PLE demonstrated adequate performance for the assessment of the depth of sedation, but it did not provide better performance than the BIS. We assumed that we could not detect differences in ability between PLE and BIS because these values and depth of sedation were evaluated 3 min after the target C_e of propofol was reached.

PLE comprises three subparameters: PLE_1 (8–32 Hz), PLE_2 (0.1–1 and 32–45 Hz), and BSR (2–32 Hz). PLE_1 and PLE_2 are calculated in the alpha (8–13 Hz) and beta (13–30 Hz) bands for 4-s epoch data without overlap; slow-frequency (0.1–1 Hz) and gamma (30–45 Hz) bands are calculated for 8-s epoch data with 50% overlap. PLE_1 reflects a light hypnotic state, whereas PLE_2 reflects a surgical hypnotic state. BSR includes two types of burst-suppression detection: portions of isoelectric EEG and/or a very low power frequency for 60 s. PLE was calculated by combining PLE_1 , PLE_2 , and BSR with appropriate weights and was linearly scaled to the range of 0–100.

In the present study, the relationship between the propofol C_e and depth of sedation was modeled. The difference between the C_{e50} value of propofol for the probability of an OAA/S score ≤ 4 and that of an OAA/S score ≤ 1 was only 1.02 $\mu\text{g/ml}$, and the therapeutic index (TI) for sedation

$$\text{TI} = \frac{C_{e50_OAA/S \text{ score of } \leq 1}}{C_{e50_OAA/S \text{ score of } \leq 4}} \text{ was } 1.37, \text{ indicating that the}$$

TI for the therapeutic range of sedation for propofol was very narrow. Propofol is widely used for sedation outside of the operating room, and many clinicians have expressed concern regarding its narrow therapeutic range that can lead to sudden deep sedation. Therefore, consciousness monitoring is required during propofol-induced sedation. Several studies have shown that

monitoring using the BIS can be effective during propofol sedation in endoscopic and radiological interventions [18–20]. The results of the present study suggest that PLE can be applied fully to monitor the depth of consciousness during propofol sedation outside of the operating room. Here, propofol-induced sedation was evaluated only in healthy adult patients undergoing upper limb surgery under a brachial plexus block. As the plasma concentrations of local anesthetics increase, systemic toxicity may occur [21] and electroencephalographic signals may be affected, especially in relation to CNS toxicity. In the present study, no patients complained of symptoms of toxicity during the procedure; therefore, we can exclude the CNS effect of local anesthetics on monitoring. However, additional clinical studies are needed with other anesthetics, as well as larger and more heterogeneous populations, in order to determine the correlation between the OAA/S score and PLE and to investigate the accuracy of PLE.

In conclusion, we observed a good correlation between PLE and the depth of sedation, as measured by the OAA/S score, during propofol-induced sedation in patients undergoing upper limb surgery under a brachial plexus block. The monitoring performance of PLE was comparable with that of the BIS, indicating that it may be useful as a consciousness monitoring system for measuring sedation levels.

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Conflicts of Interest

No potential conflict of interest relevant to this article was reported.

Author Contributions

Mi ROUNG Jun (Data curation; Formal analysis; Investigation; Validation; Writing—original draft; Writing – review & editing)
 Jae Hwa Yoo (Investigation; Validation)
 Sun Young Park (Writing—review & editing)
 Sojin Na (Data curation)
 Hyerim Kwon (Data curation)
 Jae-Hwi Nho (Investigation)
 Soon Im Kim (Conceptualization; Funding acquisition; Methodology; Supervision; Writing – original draft; Writing – review & editing)

ORCID

Mi ROUNG Jun, <https://orcid.org/0000-0003-0330-9102>
 Jae Hwa Yoo, <https://orcid.org/0000-0003-0675-0761>
 Sun Young Park, <https://orcid.org/0000-0003-2588-3324>
 Sojin Na, <https://orcid.org/0000-0003-0240-3260>
 Hyerim Kwon, <https://orcid.org/0000-0002-6241-4474>
 Jae-Hwi Nho, <https://orcid.org/0000-0003-1053-456X>
 Soon Im Kim, <https://orcid.org/0000-0001-8884-4096>

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